

X선 영상기법을 활용한 생체유동현상 계측에 관한 연구

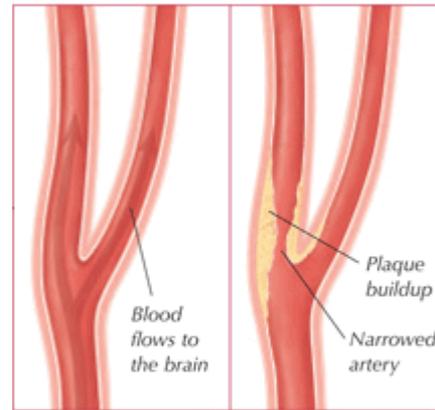
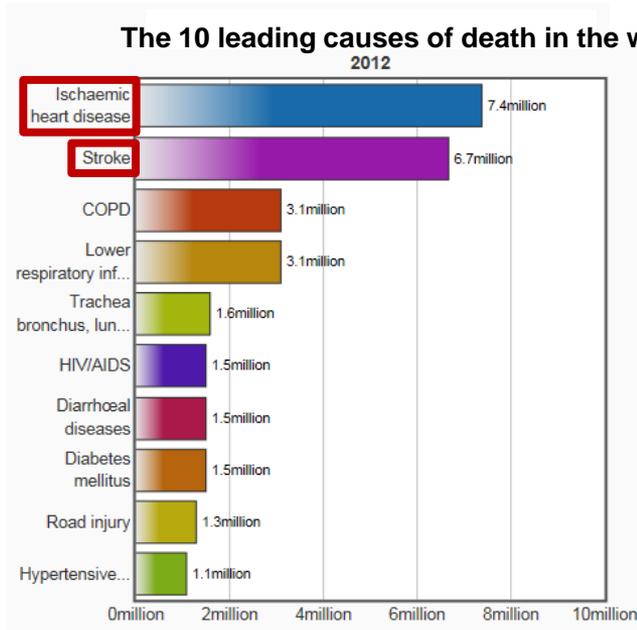
2019. 06. 22

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박한욱

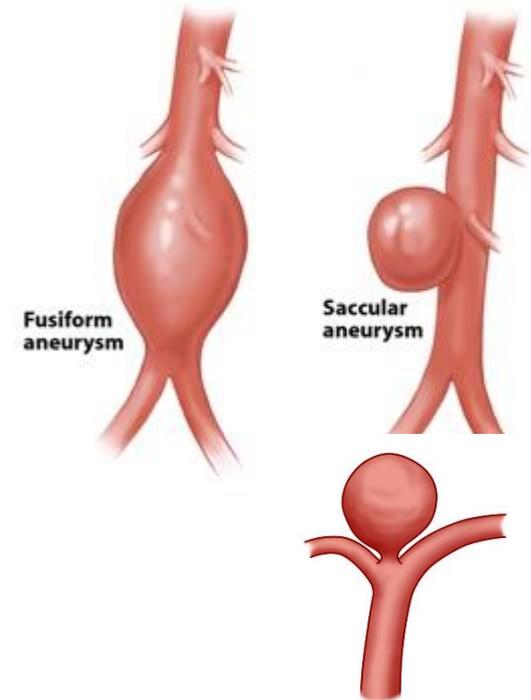
Introduction

✓ Necessity of measurement of blood flows



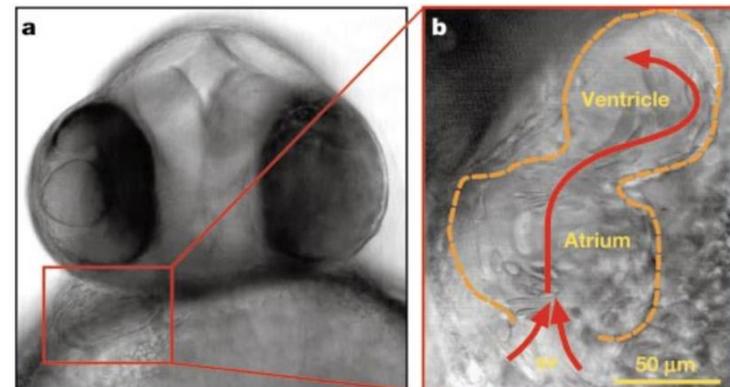
A healthy carotid artery lets blood flow easily to the brain.

Problems with blood flow can occur when an artery is narrowed by plaque.



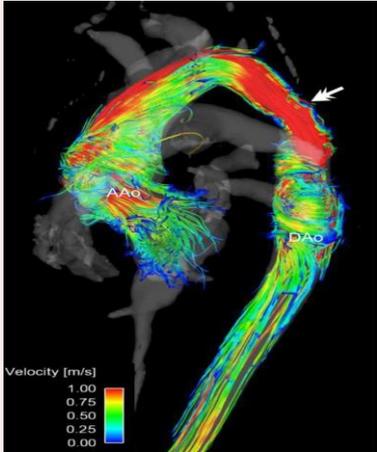
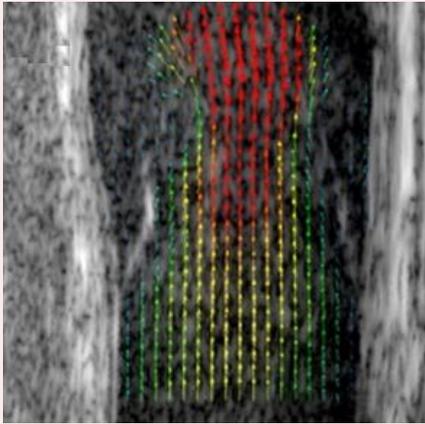
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Department of Neurosurgery

- Disorders in circulatory system
are **major mortality**.



Introduction

✓ Comparison of non-invasive technique.

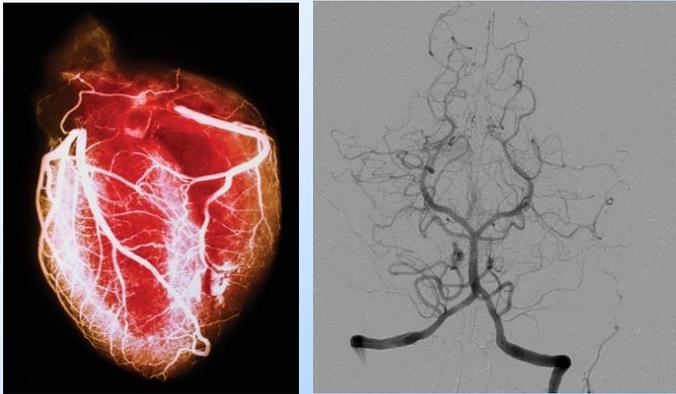
	MRI	Echo PIV	X-ray PIV
Merit	3D measurement	Portable, availability	Penetration depth, Spatial resolution
Limitation	Temporal resolution	Trade off : Penetration & temporal resolution	Availability
Application			

Introduction

X-ray PIV Technique

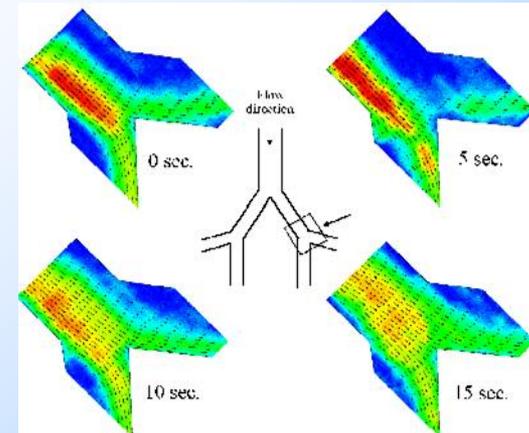
X-ray Imaging

- High resolution.
- Qualitative flow information.



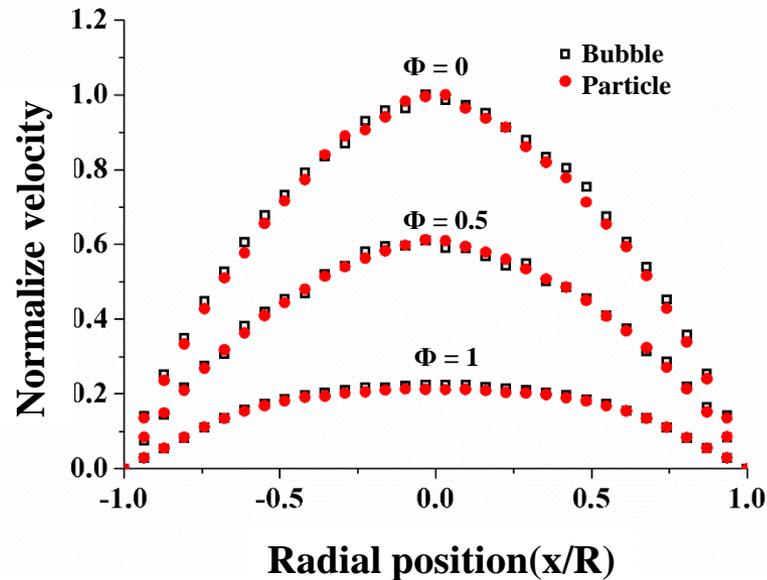
Particle Image Velocimetry

- A method of flow visualization.
- Quantitative flow information.

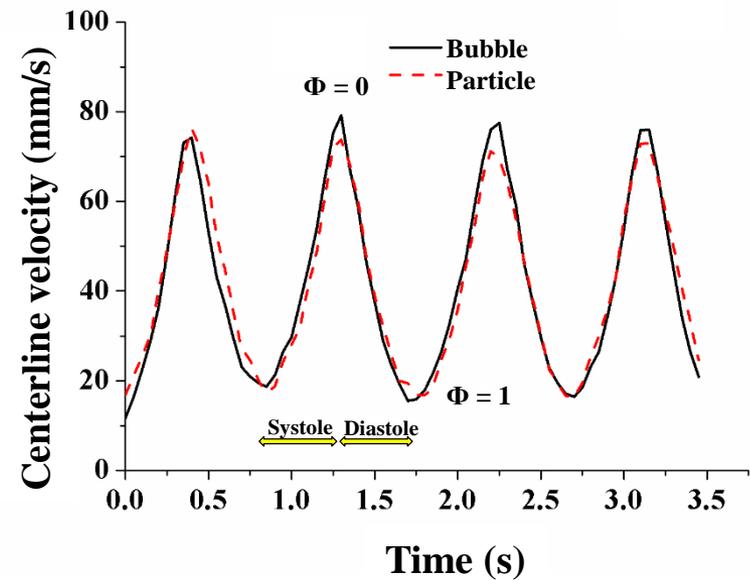


Validation of CO₂ microbubble in pulsatile flow

✓ Velocity profile of Newtonian fluid flow



Velocity profile of Newtonian fluid

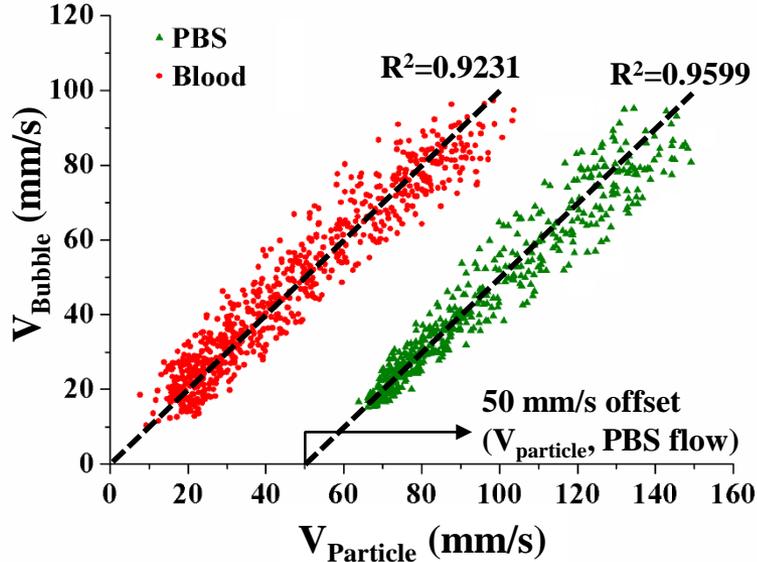


Variation of centerline velocities

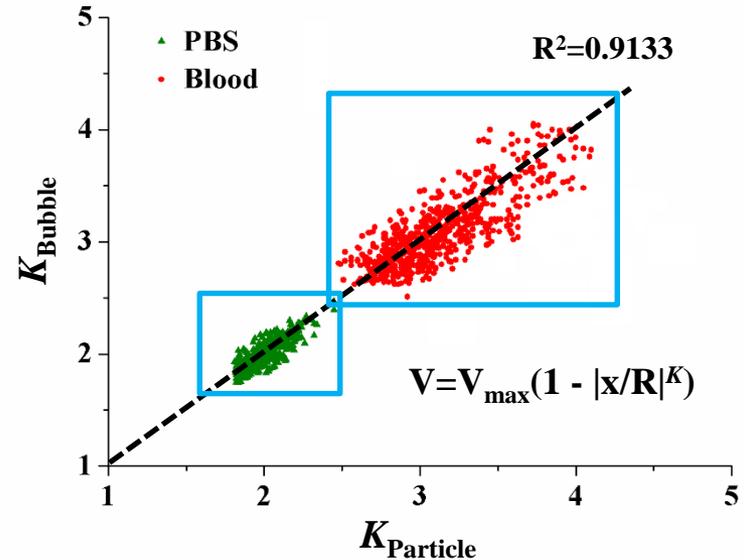
- ✓ To validate the use of CO₂ microbubbles, **the measured velocity data of the CO₂ microbubbles are compared** with those of 14 μm silver-coated hollow glass beads widely used as tracer particles in X-ray PIV experiments.

Accuracy of CO₂ microbubble in pulsatile flow

✓ Centerline velocity distribution.



✓ K -value distribution.



✓ Results at 10 phases ($\Phi = 0, 0.11, 0.22 \dots 1$) over 16 cycles were used.

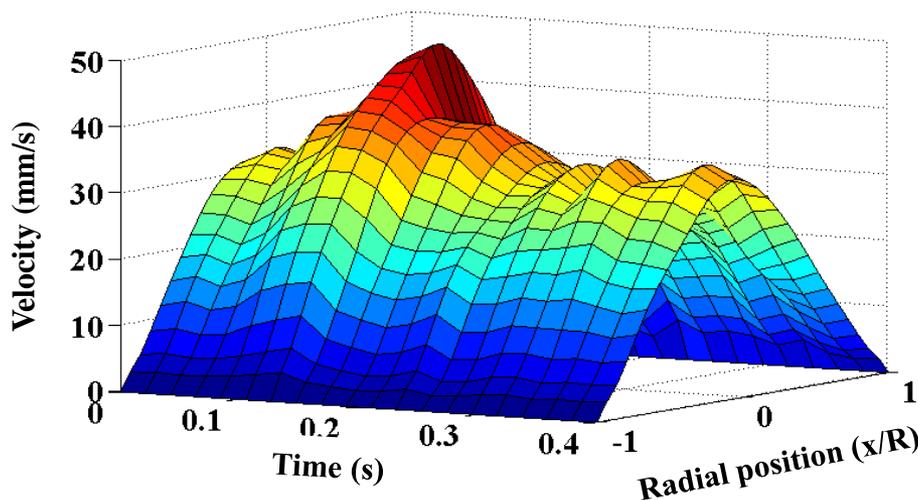
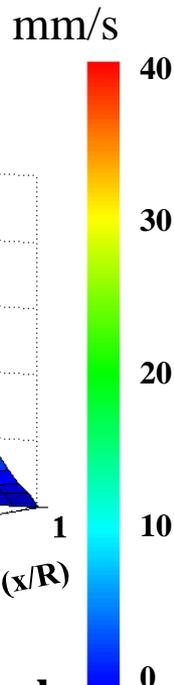
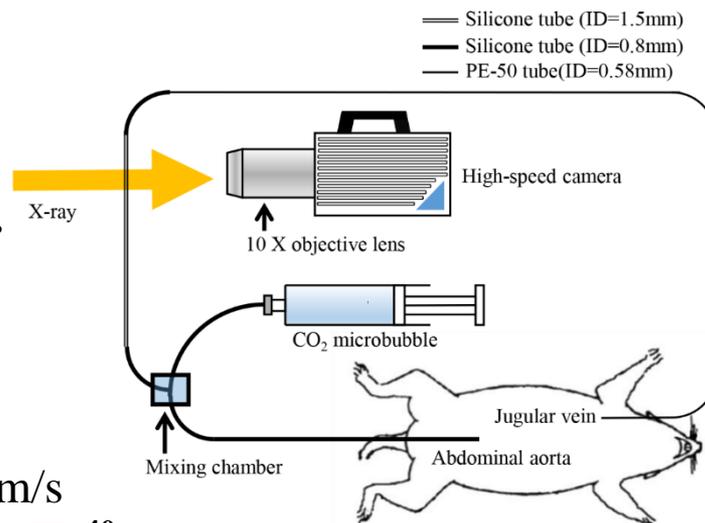
✓ Centerline velocity and K -value between CO₂ microbubbles and particles was revealed.

✓ The K -value and centerline velocity measured by CO₂ microbubble and particles was **highly correlated** with high R^2 value

Velocity information of rat extracorporeal loop

✓ Rat extracorporeal loop system

- Real **pulsatile blood flow**.
- Control velocity, flow rate and pulsatility.
- CO₂ microbubbles were used as a tracer particle.



Velocity distribution in a cardiac cycle

Results

Centerline velocity (systolic) :
47.97 mm/s

Centerline velocity (diastolic) :
23.19 mm/s

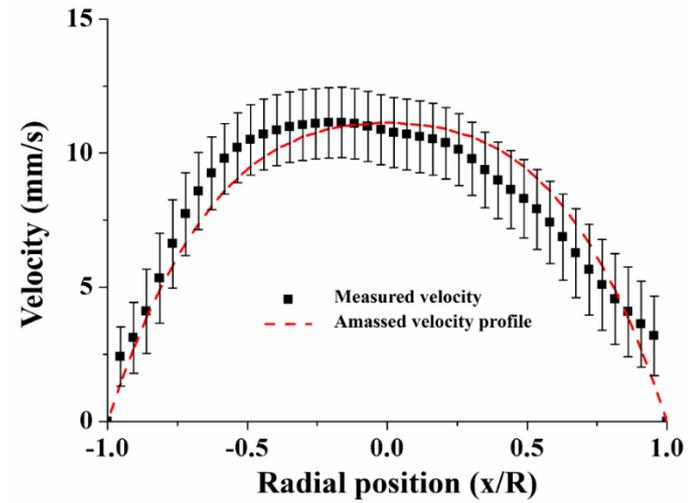
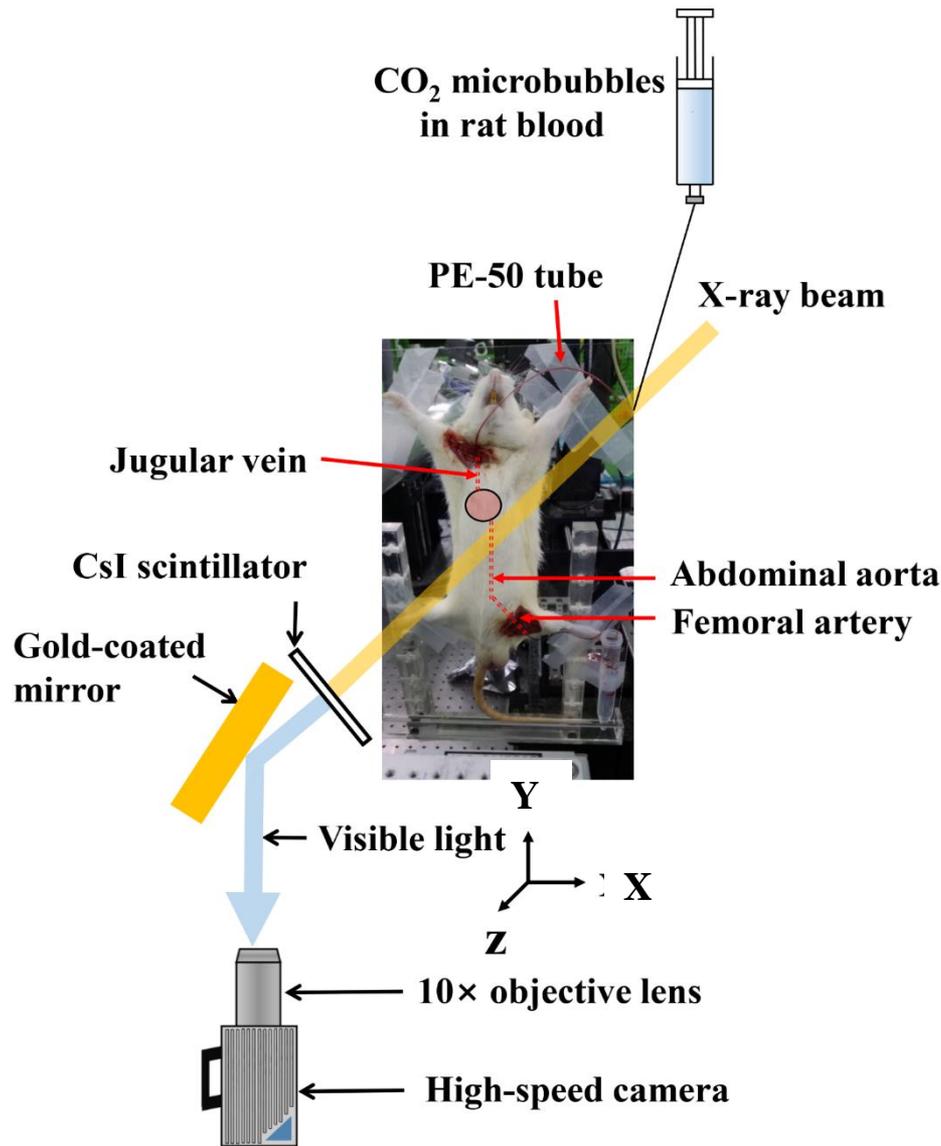
Pulsatile index : 0.7728

Heart rate : 2.53 Hz

K-value : 2.83

Flow rate : 2.3620 mL/min

Velocity profile of abdominal aorta



Velocity profile of abdominal aorta

Cadaver experiment condition

Working fluid : Blood

Particle : CO₂ bubble

1000fps

10x lens

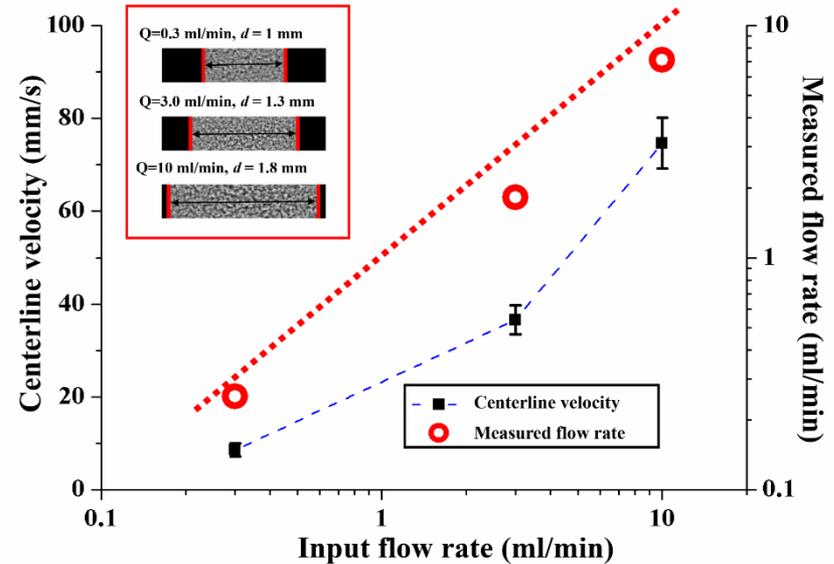
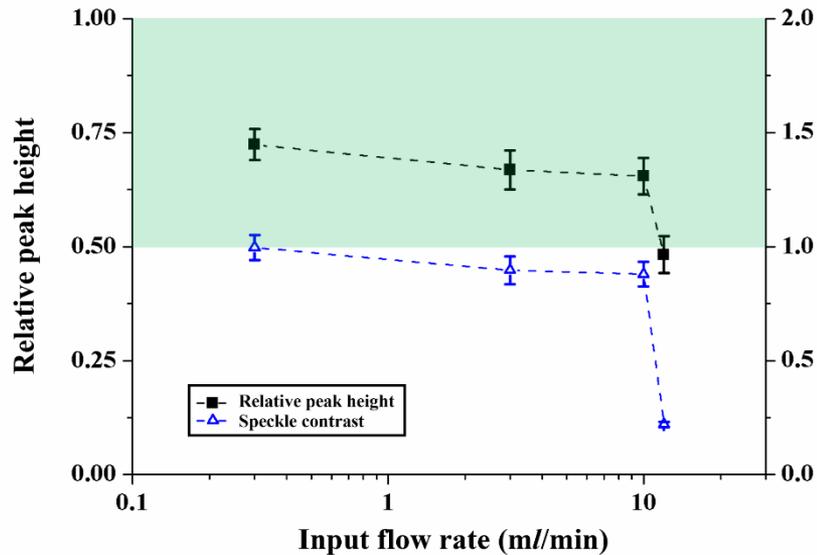
PIV condition

1024 × 1024 pixel(2.0 mm × 2.0 mm).

32 × 64 interrogation window.

50% overlapping.

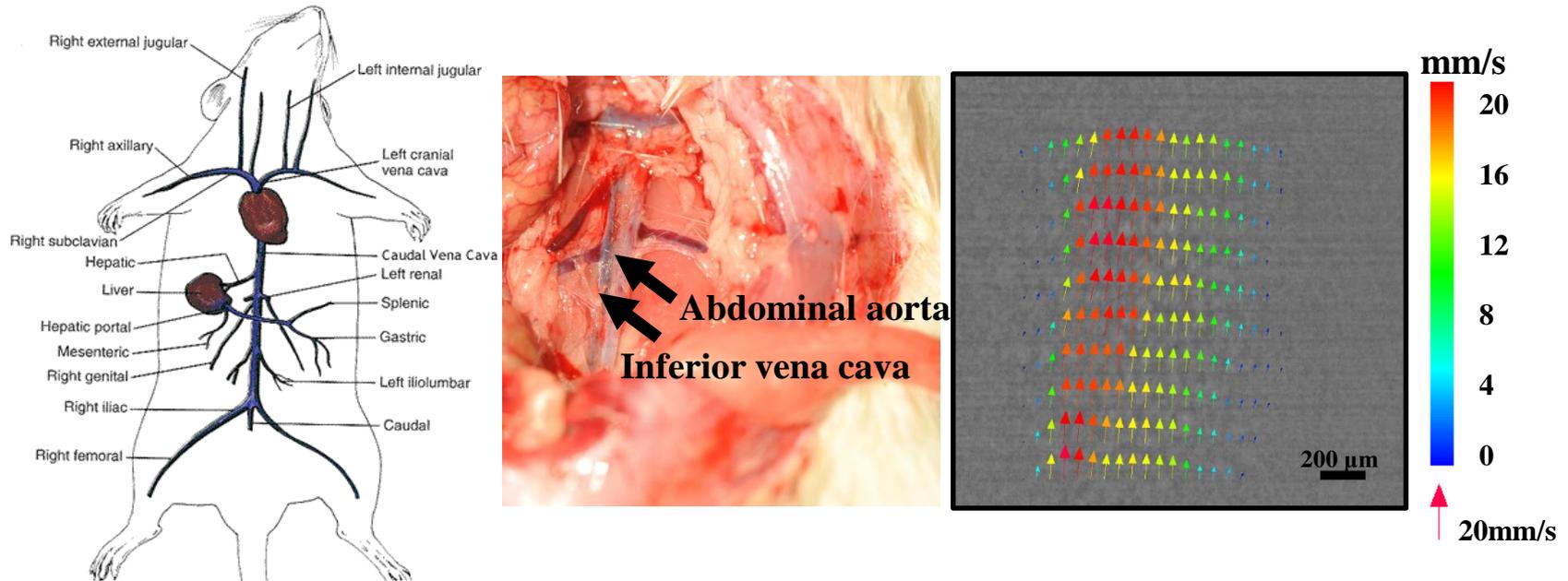
Maximum measurable velocity



1. The **maximum measurable velocity** that corresponds to the **input flow rate of 10 mL/min** should be determined.
2. The **maximum measurable blood flow rate is approximately 7.1 mL/min**, at which the **centerline velocity is 74.64 mm/s**, as determined using X-ray PIV in the rat model.

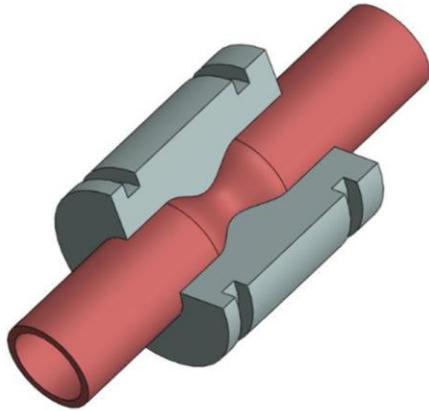
In vivo measurement of blood flow

✓ Velocity fields in interior vena cava under *in vivo* conditions



1. **The velocity fields of blood flow were measured** in the inferior vena cava (IVC) of the rat under *in vivo* conditions.
2. The present X-ray PIV technique with CO₂ microbubbles **has a strong potential in the *in vivo* measurements** of real blood flows in animal models.

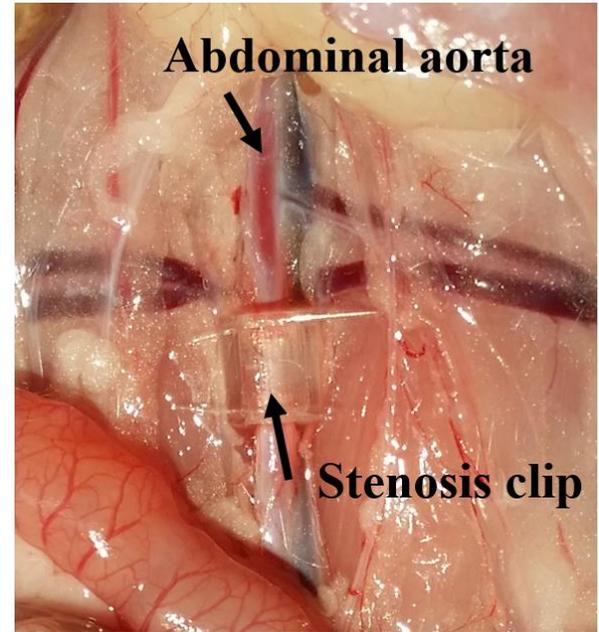
Stenosis model



3D stenosis clip installed
in a blood vessel



Abdominal aorta



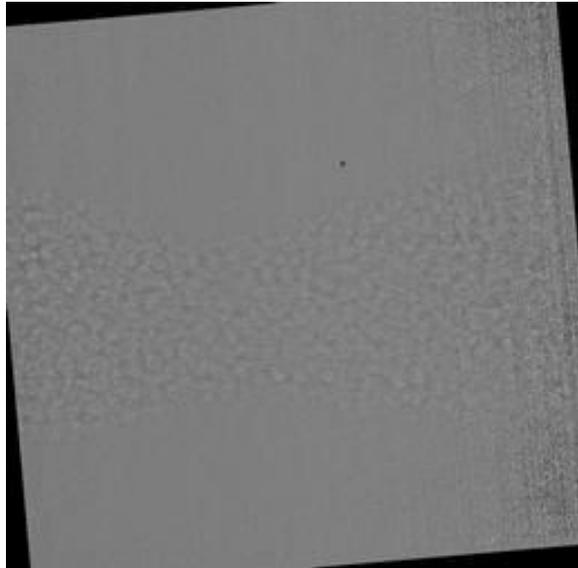
Stenosis model
at abdominal aorta

Severity S	26%	36%	54%
Inner diameter of vessel D (mm)	1.04	0.96	1.05
Radius of stenosis throat r_0 (mm)	0.77	0.614	0.484
Length of stenosis L (mm)	1.92 (1.85 D)	1.66 (1.73 D)	1.54 (1.47 D)

Geometric parameters of three stenosis clips tested in this study

Velocity field

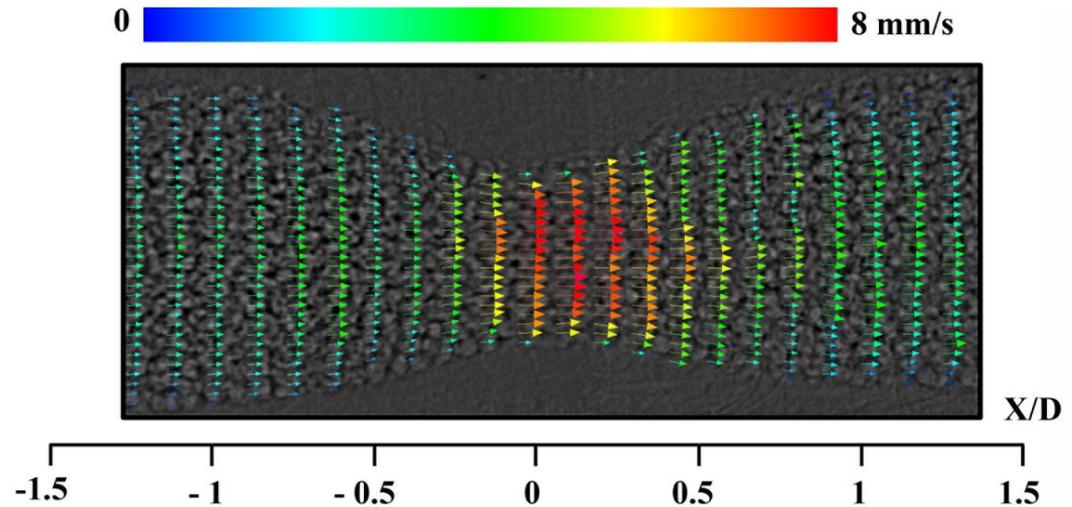
✓ Velocity field information in 36% concentric stenosis.



**X-ray images in
36% concentric stenosis**

Experiment condition

Working fluid : Blood
Particle : CO₂ microbubbles
Q = 0.5mL/min
500 fps
10x objective lens

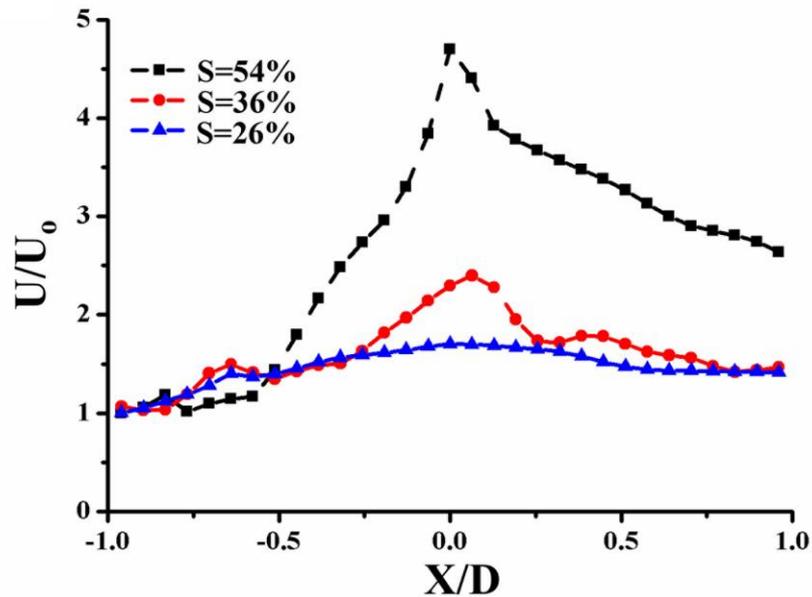


Instantaneous velocity field

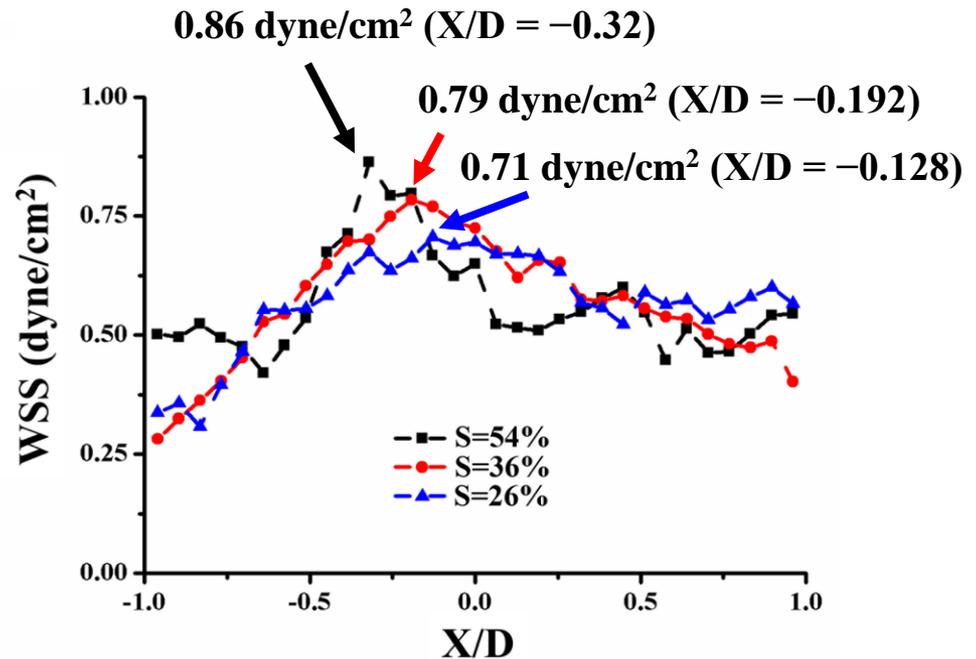
PIV condition

1024 x 1024 pixel(2 mm x 2 mm).
64 x 32 interrogation window.
50% overlapping.
Average 400 pairs of velocity field.

Velocity and WSS distribution



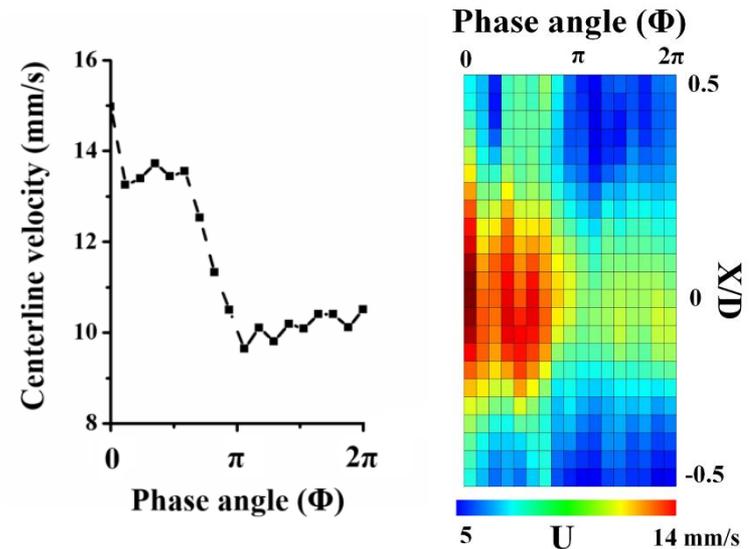
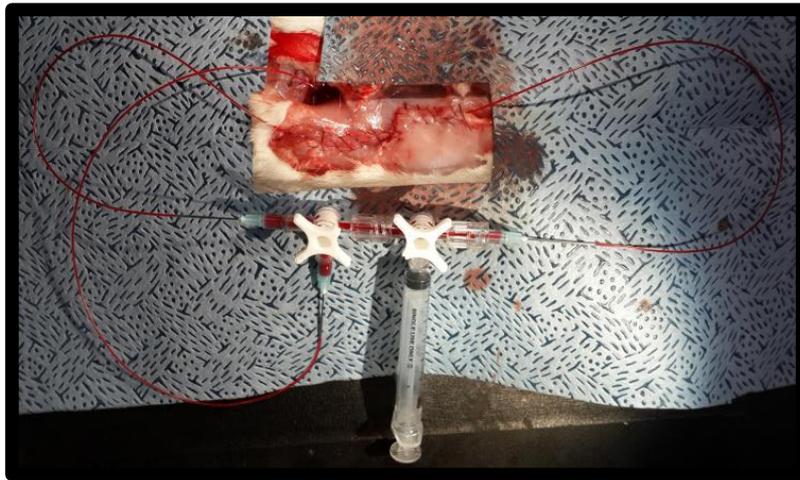
Variations in normalized velocity



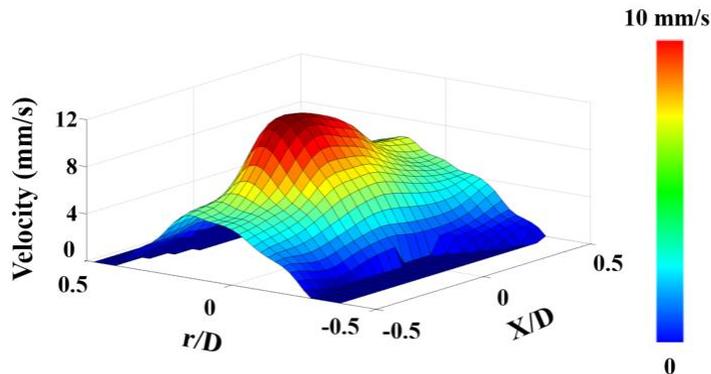
Variations in WSS

1. The peak values of WSS occurred at **locations prior to the throat of the stenosis** ($X/D < 0$) in all cases.
2. The peak location **shifted forward to the throat**, and the corresponding **WSS peak value increased** with the **increase in stenosis severity**.

Hemodynamic information on *in vivo* model



Rat stenosis model for *in vivo* measurement



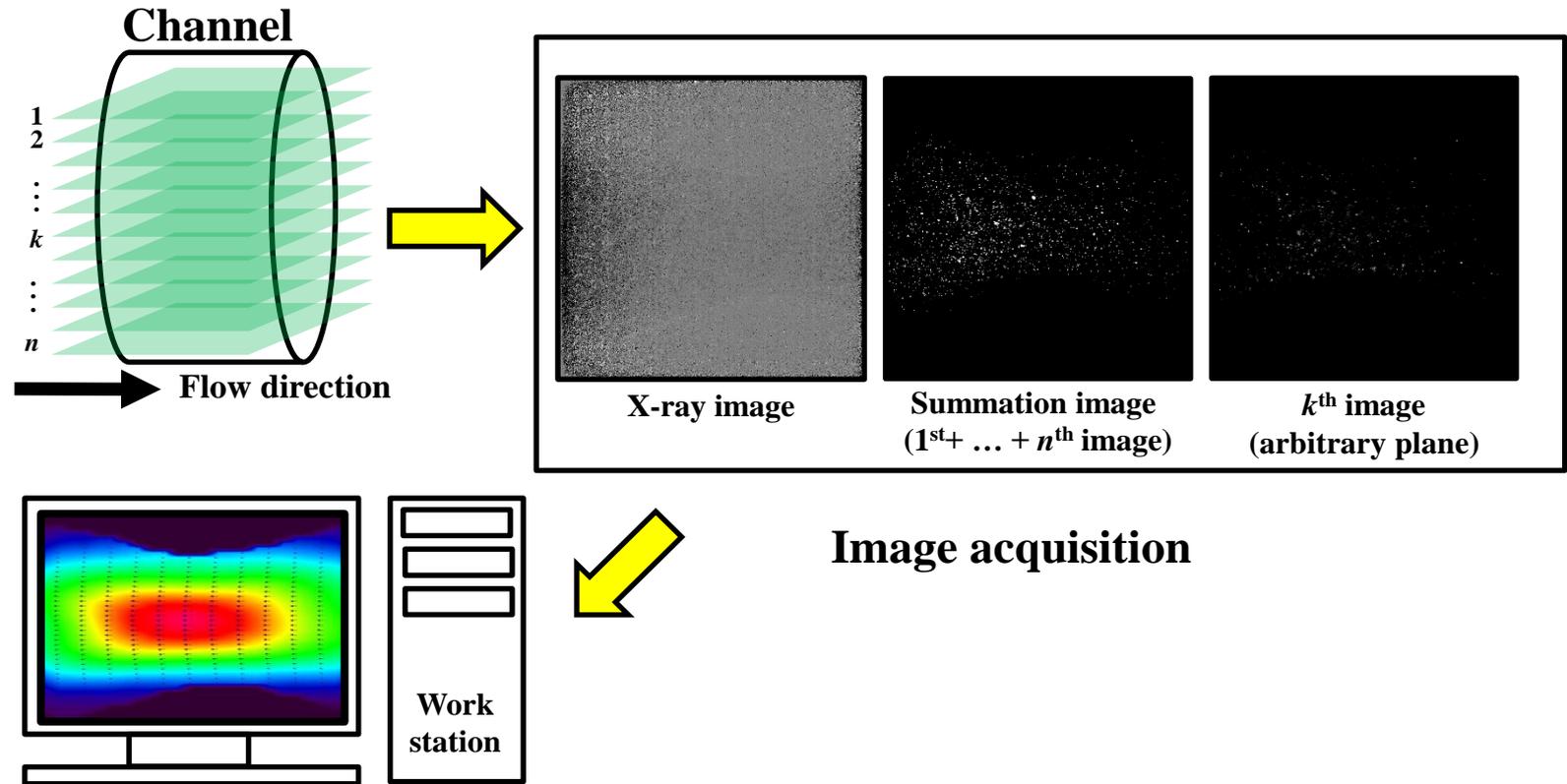
Variation in radial velocity profile in stenosis

Phasic variation and vibration in centerline velocity

Results

Centerline velocity (systolic) : 14.97 mm/s
Centerline velocity (diastolic) : 10.51 mm/s
Pulsatile index : 0.43
Heart rate : 1.35 bpm

Objective & theoretical background

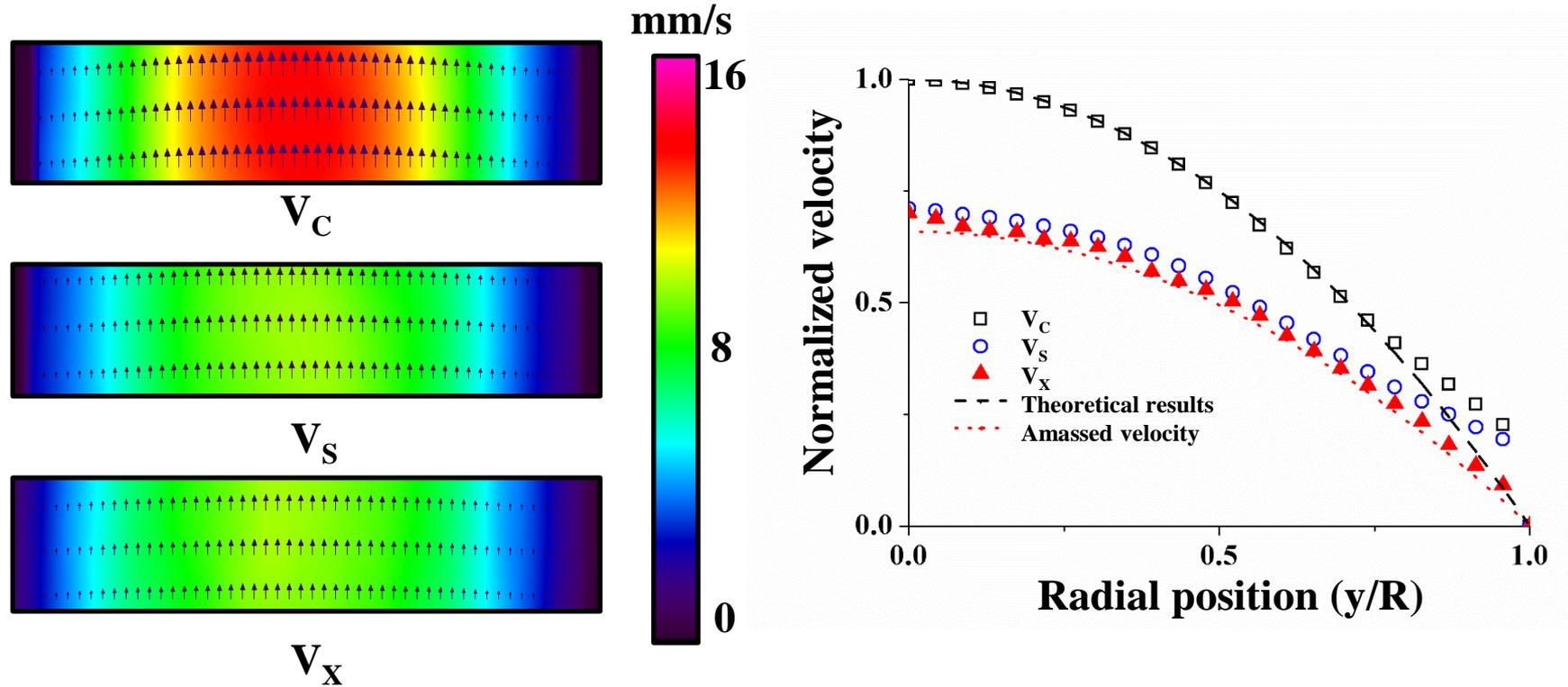


PIV (two-frame cross correlation)

1. Identify the **similarity of V_x and V_s** and confirm the **relationship between I_s, I_k** .
2. **Find correction coefficients for every I_k** and apply them to X-ray PIV results.

Results

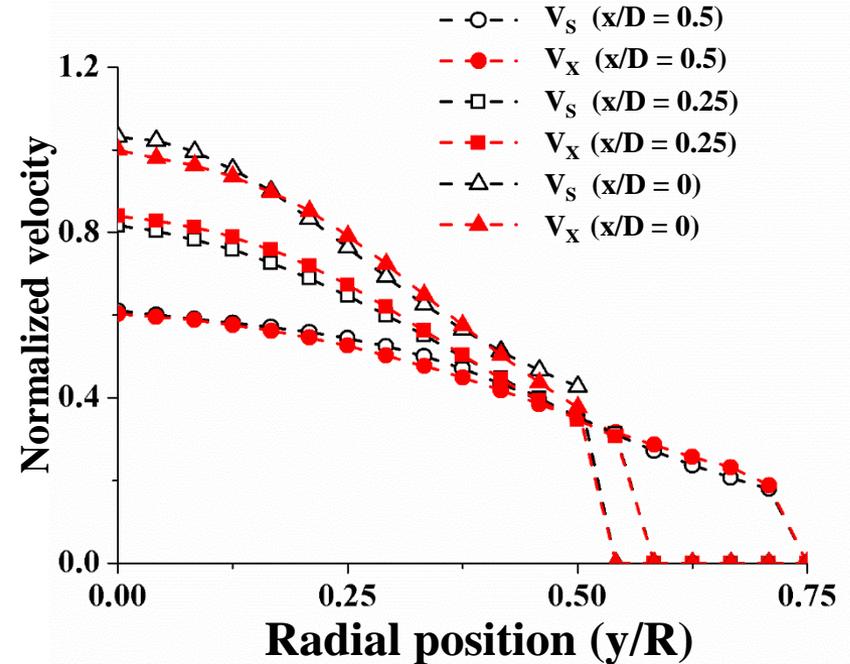
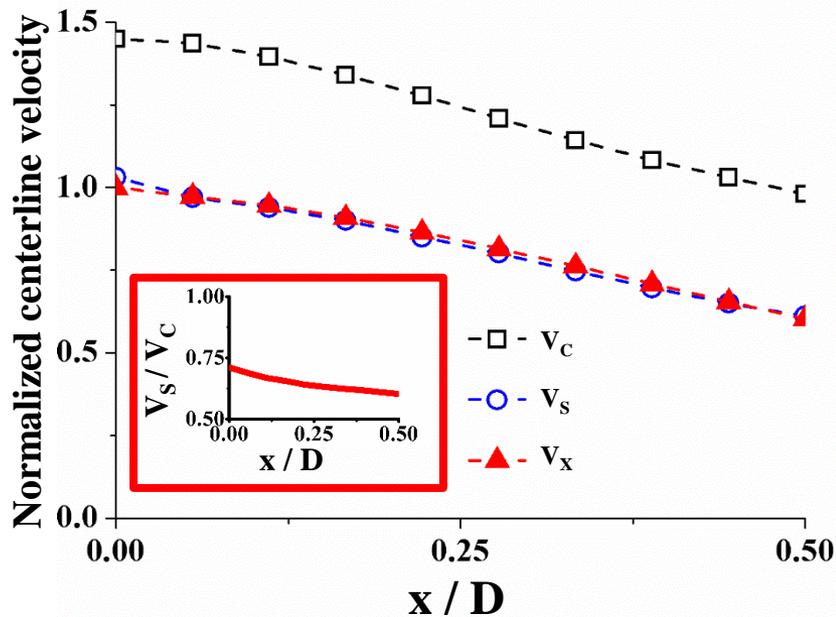
✓ Velocity information in Poiseuille flow



1. Velocity information (V_C , V_S , V_X) were directly compared in this study.
2. The **measurement accuracy** of X-ray PIV was **constant throughout the radial direction**.

Results

✓ Velocity information of flow in the 50% concentric stenosis



1. Different from the constant value ($2/3$) for the Poiseuille flow, **the correction coefficient gradually decreased as the x/D increases.**
2. Except in the near-wall region, **the velocity information of V_X and V_S are well matched** in both Poiseuille flow and flow in the stenosis with 50% severity.

Conclusion

- 1. X-ray PIV technique with hollow CO₂ microbubbles were employed to investigate hemodynamic characteristic of blood flows.**
- 2. The traceabilities of CO₂ microbubbles in steady and pulsatile blood flows were demonstrated.**
- 3. The feasibility of CO₂ microbubbles streaming in a live rat model with real surrounding tissues after applying digital image processing was also demonstrated.**
- 4. The direct comparison of the experimental data measured by the proposed X-ray PIV technique with those of micro-PIV technique demonstrated improvement in measurement performance.**
- 5. The hemodynamic information of blood flows in the stenosed vessel of a rodent model was obtained using X-ray PIV.**

Thank you